



**UNITED REPUBLIC OF TANZANIA**

**MINISTRY OF HEALTH**



**TANZANIA MEDICINES AND MEDICAL DEVICES AUTHORITY**

**GUIDANCE ON THE QUALITY AND CLINICAL REQUIREMENTS FOR  
INHALATION AND NASAL MEDICINAL PRODUCTS**

*(Made under Regulation 4 (1) of the Tanzania Medicines and Medical Devices (Registration of Medicinal Products) Regulations, 2015*

**October, 2023**

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## ABBREVIATION OF TERMS

<b>API</b>	- Active Pharmaceutical Ingredient
<b>APSD</b>	- Aerodynamic Particle Size Distribution Breath Operated Inhaler
<b>AUC</b>	- Area under the plasma concentration curve
<b>BOI</b>	- Breath Operated Inhaler
<b>BP</b>	- British Pharmacopeia
<b>C<sub>max</sub></b>	- Maximum or peak plasma concentration
<b>DD</b>	- Delivered Dose
<b>DPI</b>	- Dry Powder Inhaler
<b>EMA</b>	- European Medicines Agency
<b>FPD</b>	- Fine Particle Dose
<b>FPM</b>	- Fine Particle Mass
<b>GSD</b>	- Geometric Standard Deviation
<b>MMAD</b>	- Mass Median Aerodynamic Diameter
<b>OIP</b>	- Orally Inhaled Products
<b>PD</b>	- Pharmacodynamic
<b>PK</b>	- Pharmacokinetic
<b>pMDI</b>	- Pressurised Metered Dose Inhaler
<b>T<sub>max</sub></b>	- Time to C <sub>max</sub>
<b>TMDA</b>	Tanzania Medicines and Medical Devices Authority
<b>UDD</b>	- Uniformity of Delivered Dose
<b>USP</b>	- United States Pharmacopeia
<b>WHO</b>	- World Health Organization

## **ACKNOWLEDGEMENTS**

This guidance has been developed by technical Experts who worked tirelessly in crafting and finalizing this document. Special gratitude is bestowed upon the following Experts: -

- Mr. Felchism Apolnary;
- Mr. Denis Mwangomo;
- Mr. Jackson Kiberenge;
- Dr. Athanas Mseki; and
- Ms. Sarah Mamkwe.

I would further like to thank Mr. Salum Mkata, a Pharmaceutical Science Tutor from Nobo College of Pharmacy who served as an external consultancy during the development of the guidance.

My special appreciation is extended to the European Medicines Agency (EMA), World Health Organization (WHO), and US Food and Drug Administration (FDA) whose documents served as references during the development of this guidance.

Lastly, the TMDA Management team is acknowledged for their constructive inputs and endorsement of the guidance document.

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**DIRECTOR OF HUMAN AND VETERINARY MEDICINES**

## **GLOSSARY OF TERMS**

For the purpose of this guidance the following terminologies are applicable.

### **Comparator product**

Means a pharmaceutical product with which the generic product is intended to be interchangeable in clinical practice. The comparator product will normally be the innovator product for which efficacy, safety and quality have been established.

### **Delivery device**

Means the sum of component(s) of the container closure system responsible for delivering the drug to the respiratory tract (inhalation product) or the nasal and/or pharyngeal region (nasal product).

### **Extractables**

Means the compounds which may be extracted from the container closure system by using stressful conditions.

### **Fine particle dose (FPD) or Fine Particle Mass (FPM)**

Means the same amount of particles  $\leq 5\mu\text{m}$  per actuation/puff or dose that are delivered to the lung.

### **Generic product**

Means a medicinal product which has the same qualitative and quantitative composition in active substances and the same pharmaceutical form as the reference medicinal product, and whose bioequivalence with the reference medicinal product has been demonstrated by appropriate bioavailability studies.

### **Inhalation medicine**

Means a drug product (including the delivery device, where applicable) whose intended site of deposition is the respiratory tract. The site of action may be local or systemic.

### **Leachable**

Means the compounds which may leach from the container closure system into the formulation under normal conditions of storage and use.

**Spacer**

Means a spacing device and is also known as a valved holding chamber. It aids inhalation.

**Strength/dose**

Means an amount of drug that is metered in the device for a single inhalation manoeuvre whereas a single dose may contain for example 2 puffs of a pMDI or 4 puffs of a pMDI. So, for example, for doses of 12µg and 24µg formoterol pMDI one and 2 puffs of the 12µg strength or two puffs of both the 6µg and 12µg strength might be used.

**Pulmonary deposition**

Means an amount of active substance deposited in the airways (mouth and throat excluded).

## **FOREWORD**

This is the first edition of the guidance on the quality and clinical data requirements for inhalation and nasal products. The guidance also provides specific requirements for variations to existing medicines. The document aims to guide applicants on the quality and clinical data requirements that should be submitted to support marketing authorization of nasal spray and inhalation medicinal products.

The use of inhaled drug products, such as metered dose inhalers (MDIs) and nasal dry powder inhalers (DPIs), is becoming increasingly common despite the known challenge of ensuring uniform dose delivery. The effectiveness of these products depends not only on the formulation but also on the delivery device and the patients' experience, including coordination skills during their use.

Due to the complexity in their delivery, predicting clinical outcomes has been challenging. The published TMDA's Compendium Guidelines for Marketing Authorization of Medicinal Products does not fully address the specific issues relating to these products.

This document addresses specific issues relevant to medicinal products and delivery devices but may not be able to offer complete guidance on every aspect of the quality and clinical documentation for the product. Therefore, this guidance should be read in conjunction with other relevant guidelines cited in this guidance.

It is anticipated that this document will provide guidance to applicants to prepare and compile complete documents to support their applications for marketing authorization. This will facilitate efficient review and avoid queries that result in unnecessary delays in the approval of the medicines, thus improving access to quality, safe, and efficacious assured medicines for patients.

**Adam M. Fimbo**  
**DIRECTOR GENERAL**

1 **1. INTRODUCTION**

2  
3 **1.1 Background**

4  
5 Nasal spray and inhalation products are used to treat respiratory infections and lung  
6 diseases characterized by airflow obstruction and shortness of breath, including asthma,  
7 chronic obstructive pulmonary disease (COPD), and cystic fibrosis.

8  
9 These dosage forms have unique characteristics as their performance is dependent not  
10 only on the active pharmaceutical ingredient and excipients but also on the container  
11 closure system, including delivery devices such as the valve and metered system. The  
12 products are designed to deliver the active ingredients to the nasal mucosa, pharyngeal  
13 region, and lungs.

14 The intended site of action of the active ingredient can be local or systemic:

- 15 i. Inhalation medicines are intended to be deposited in the respiratory tract.  
16 ii. Nasal spray medicines are intended to be deposited in the nasal or pharyngeal  
17 region.

18 Inhalation and nasal spray medicines typically exhibit more variable bioavailability  
19 compared to medicines administered through other routes due to the variability in usage,  
20 such as the patient's inspiratory flow pattern.

21 This document provides guidance to applicants on the quality and clinical data  
22 requirements that should be submitted to support the marketing authorization of nasal  
23 spray and inhalation medicinal products, including variations to existing medicines. It  
24 covers both single active pharmaceutical ingredient products and combination products.

25 Furthermore, this guidance addresses specific issues related to the performance of  
26 delivery devices. Given the wide diversity of inhalation and nasal products in terms of  
27 delivery devices, applicants are expected to refer to other relevant references, such as  
28 the United States Pharmacopeia, European Pharmacopoeia, and ISO standards.

29  
30 **1.2 Scope**

31  
32 The scope of this guidance encompasses products that are intended to administer the  
33 active pharmaceutical ingredient to the lungs, nasal mucosa, and pharyngeal region. This  
34 includes various delivery systems such as pressurized metered dose inhalers, dry powder  
35 inhalers, nebulization products, non-pressurized metered dose inhalers, pressurized  
36 metered dose nasal sprays, and nasal powders.

37 It's important to note that this guidance does not apply to systemically acting medicines,  
38 liquid inhalation anesthetics, nasal ointments, creams, and gels. These types of products  
39 are not within the scope of this particular guidance document.



41 **2. QUALITY**

42

43 **2.1 Quality guidelines**

44

45 Specific guidelines that should be referred to for the quality requirements of inhalation  
46 and nasal products include:

47 i. Guideline on the pharmaceutical quality of inhalation and nasal products  
48 (EMA/CHMP/QWP/49313/2005 Corr);

49

50 ii. WHO Guideline on stability testing of active pharmaceutical ingredients and  
51 finished pharmaceutical products (WHO Technical Report Series, No. 1010,  
52 Annex 10, 2018);

53

54 iii. Guideline on process validation for finished products – information and data to be  
55 provided in regulatory submission (EMA/CHMP/CVMP/QWP/BWP/70278/2012-  
56 Rev1).

57

58 In addition to the above guidelines, applicants are advised to refer to the following  
59 pharmacopeia general monograph and chapters:

60 i. The BP general monograph for Preparations for Inhalation;

61

62 ii. USP general monograph <5> Inhalation and nasal drug products—general  
63 information and product quality tests;

64

65 iii. USP chapter <610> Inhalation and Nasal Drug Products: Aerosols, sprays, and  
66 Powders – Performance Quality Tests;

67

68 Note: the current version of the referenced documents should be used during the  
69 application process, and any changes to the reference documents should also be applied  
70 to applications for registration submitted to TMDA.

71

72 **2.2 Delivery devices**

73 The development of the delivery device should be thoroughly described. Any changes  
74 made in the design, such as modifications to component materials, or manufacturing  
75 process, such as scaling up from single cavity to multiple cavity tooling, during the product  
76 development should be discussed in terms of their impact on the performance  
77 characteristics of the product. This includes parameters (e.g., delivered dose, fine particle  
78 mass, etc.).

79 To demonstrate the equivalence of the comparator product with the product intended for  
80 marketing, appropriate comparative data on the generic product should be provided.

81 For device-metered dry powder inhalers, measures should be in place to prevent  
82 unintentional multiple dose metering and subsequent inhalation by the patient. Data  
83 should be provided to demonstrate that all target patient groups are capable of triggering  
84 the delivery device in breath-activated devices. This can be evaluated as part of the  
85 clinical program during patient handling studies. The triggering mechanism should be  
86 well-characterized as part of the delivery device development program.

87 For device-metered dry powder inhalers, each unit should have a counter or other fill  
88 indicator to provide the patient with an indication of when the number of actuations stated  
89 on the label has been delivered. Including dose counters is also encouraged for other  
90 multiple dose products.

91

### 92 **2.2.1 Rubber or plastic in delivery devices**

93

94 The following additional information should be provided: -

95

- 96 i. Identify each material, the formulation code and the manufacturer
- 97 ii. Include evidence of the biological safety of all components
- 98 iii. Provide test certificates or reports to demonstrate compliance if the evidence refers  
99 to a monograph in a recognized pharmacopoeia
- 100 iv. Include details of any extractable or leachable studies performed if your product  
101 contains a liquid or gas, because substances can leach from rubber or plastic  
102 material in valve components or gaskets of delivery devices (in Module 3.2.P.2.4).  
103 For more information, go to EMEA/CHMP/QWP/49313/2005 Corr Section 4.2.1.3.

104 This information should be provided in section 3.2.P.2.4 (selection of container closure)  
105 and 3.2.P.7 (container closure system).

106

### 107 **2.2.2 Colour of delivery devices**

108

109 If the colour of the delivery device is not similar to that of the comparator product:

110

- 111 i. Provide a clinical justification for the colours used
- 112 ii. Discuss safety issues around how a user will recognise the difference between  
113 different medicines.

114

### 115 **2.2.3 Counters**

116

117 Counters and fill indicators let the user know when they need to replace the inhaler.

118

- 119 i. If the comparator product has a counter or fill indicator, then a generic product  
120 needs to have one too

- 121 ii. If the comparator product does not have a counter or fill indicator, then the generic  
122 product does not need to have one, although it is recommended to include a  
123 counter or fill indicator for all multiple dose inhalation medicines.  
124

### 125 **3. REQUIREMENTS FOR DEMONSTRATION OF THERAPEUTIC EQUIVALENCE** 126

127 This section outlines the requirements for designing, conducting, and evaluating the  
128 therapeutic equivalence of inhalation and nasal products. The data provided should  
129 demonstrate the equivalence between the comparator product and the generic product,  
130 aiming to establish the safety and efficacy of the product intended for marketing  
131 authorization.  
132

133 For generic products to be considered acceptable, they must be of satisfactory quality  
134 and therapeutically equivalent to the comparator product in terms of the following aspects:  
135

- 136 i. Dosage forms;
  - 137 ii. Strengths; and
  - 138 iii. Indications and directions for use.
- 139

#### 140 **3.1 Choice of the comparator product** 141

142 For in-vitro, pharmacokinetic and clinical efficacy studies of inhalation products and nasal  
143 medicines, the acceptable comparator product should be used.  
144

145 General principles for the selection of comparator products are described in the Annex IV  
146 of Compendium of Guidelines for Marketing Authorization of Human Medicinal Products,  
147 1st revision, July, 2020: *Selection of a comparator product to be used in establishing*  
148 *interchangeability*.  
149

#### 150 **3.2 Therapeutic equivalence guidelines** 151

152 Due to the complexity of the formulation and method of administration, specific studies  
153 are necessary to demonstrate the therapeutic equivalence between the comparator  
154 product and the generic formulation of inhalation and nasal products. To establish this  
155 equivalence, the following specific guidelines should be consulted:

- 156 i. Guideline on the requirements for clinical documentation for orally inhaled products  
157 (OIP) including the requirements for demonstration of therapeutic equivalence  
158 between two inhaled products for use in the treatment of asthma and chronic  
159 obstructive pulmonary disease (COPD) in adults and for use in the treatment of  
160 asthma in children and adolescents (CPMP/EWP/4151/00 Rev 1);  
161

- 162 ii. Note for guidance on the clinical requirements for locally applied, locally acting  
163 products containing known constituents (CPMP/EWP/239/95); and  
164  
165 iii. Questions and Answers: positions on specific questions addressed to the  
166 Pharmacokinetics Working Party (EMA/618604/2008 Rev. 13): Question 17  
167 Evaluation of orally inhaled medicinal products.

168 The above guidelines are not exhaustive, therefore other recognized publication or other  
169 relevant references may be used. Furthermore, any changes to the reference documents  
170 shall also apply to applications for registration submitted to TMDA.  
171

### 172 **3.3 Specific requirements**

173

#### 174 **3.3.1 Metered-dose nasal sprays, solutions**

175

176 Demonstrate similarity between the proposed product and the comparator products by  
177 the following parameters:

178

- 179 i. Qualitative and quantitative formulation, as described for inhalation medicine  
180 solutions;
- 181 ii. Droplet size distribution, including data to show the fraction of droplets under 10  
182  $\mu\text{m}$  is very small;
- 183 – Do not use an impactor that only measures droplets smaller than 12  $\mu\text{m}$ ,  
184 because most of the droplets will be larger than 12  $\mu\text{m}$ ;
- 185 iii. Delivered dose and delivered volume; and  
186 iv. Spray times, spray pattern and plume geometry.

187 These should be generated using validated methods.

188

#### 189 *Droplet size for local effects*

190

191 When the medicine is intended to have local effects, the droplets for nasal spray  
192 medicines should generally be larger than 10  $\mu\text{m}$ . This prevents unwanted deposition in  
193 the lower airways.

194

195 It should be demonstrated that, the droplet size distribution of the aerosol cloud is  
196 appropriate for nasal administration and the number of droplets below 10  $\mu\text{m}$  is low and  
197 controlled. In addition, smaller droplets deposit in the nasal cavity may be demonstrated,  
198 depending on the velocity and direction of the aerosol cloud.

199

200

201

202

203 *Droplet size for systemic absorption*

204

205 When the medicine is intended for systemic absorption, the optimal droplet size is about  
206 5 µm for nasal spray solutions or suspensions. This gives good distribution in the nasal  
207 area and slow clearance.

208

### 209 **3.3.2 Metered-dose nasal sprays, suspensions**

210

211 All prescribed requirements under metered-dose nasal spray solutions are applicable for  
212 metered-dose nasal sprays, suspensions. Additionally, it is necessary to establish that  
213 both the proposed and comparator products have the same solid state properties as  
214 follows: -

215

216 i. Particle size distributions of the suspended active pharmaceutical ingredient within  
217 the droplets - if any of the excipients are also in suspension, the test method need  
218 to be able to distinguish between particles of the active pharmaceutical ingredient  
219 and particles of excipients; and

220

221 ii. Morphology of the particles of active pharmaceutical ingredient within the droplets

222

223 Several methods can be used to determine the particle size distribution and morphology,  
224 including:

225

226 a) laser diffraction;

227 b) optical microscopy (with or without a polarising filter or a dye, which can often  
228 distinguish between active pharmaceutical ingredient and carrier);

229 c) Raman microscopy; and

230 d) scanning electron microscopy, with or without energy-dispersive X-ray  
231 spectroscopy (EDS), which can often distinguish between active pharmaceutical  
232 ingredient and carrier.

233

### 234 **3.3.3 Solutions for nebulisation**

235

236 Physicochemical properties of solution for nebulization i.e., pH, buffer capacity, density,  
237 surface tension, viscosity and osmolality a significant impact on the deposition and  
238 absorption characteristics of the product. These properties can ultimately affect the safety  
239 and efficacy of the medication. Therefore, it is crucial to conduct a detailed analysis to  
240 ensure that the physicochemical properties of the proposed formulation are similar to  
241 those of the comparator product formulation. To assess the physicochemical properties,  
242 a validated analytical method should be employed.

243

244 When the generic product is an aqueous solution for nebulization, intended to be  
245 administered with essentially the same device, contain the same API(s) in the same

246 concentration and contain the same excipients in similar concentrations as the  
247 comparator product the requirement for *in vitro and/or in vivo* therapeutic equivalence  
248 studies may be waived.

249

### 250 **3.3.4 Suspensions for nebulisation**

251 For suspensions intended for nebulization, it is necessary to provide data demonstrating  
252 the similarity between the proposed product and the comparator product in the following  
253 aspects:

- 254 i. Qualitative and quantitative formulation: the formulation contains the same API(s)  
255 in the same concentration and contain the same excipients in similar  
256 concentrations as the comparator;
- 257 ii. Particle morphology of the active pharmaceutical ingredient in the suspension;
- 258 iii. Particle size distribution of the active pharmaceutical ingredient in the suspension:  
259 the test method needs to be able to distinguish between particles of the active  
260 pharmaceutical ingredient and particles of excipients if any of the excipients are  
261 also in suspension; and
- 262 iv. Droplet size distribution of the nebulised droplets: use appropriate methods to test  
263 droplet size.

264

### 265 **3.3.5 Metered-dose inhalation medicinal products**

266

267 For metered-dose inhalation medicinal products, the therapeutic equivalence should be  
268 demonstrated in a stepwise approach. These major steps include *in vitro* equivalence  
269 studies (step 1), pharmacokinetic studies (step 2) and pharmacodynamic studies/ clinical  
270 studies (step 3). Therapeutic equivalence is established if the requirements of one “step”  
271 are fully met.

272

#### 273 **3.3.5.1 Step 1: *In vitro* Studies**

274 For generic products, therapeutic equivalence can be established based on the fulfillment  
275 of the *in vitro* studies acceptance criteria established in the guidelines  
276 (CPMP/EWP/4151/00 Rev 1).

277

278 *In vitro* studies might be sufficient for generic product containing known active  
279 pharmaceutical ingredient criteria. The following criteria are applicable for establishing  
280 equivalence with respect to *in vitro* studies data:

281

- 282 i. The drug product contains the same active pharmaceutical ingredient as the  
283 reference product in terms of the salt, ester, hydrate, solvate etc.;
- 284 ii. The pharmaceutical dosage form is identical;

- 285           iii. In case where the active pharmaceutical ingredient is in the solid state, i.e., as a  
286           powder or suspension, different crystalline structures and/ or different polymorphic  
287           forms should do not affect the product performance;  
288           iv. Qualitative and/ or quantitative differences in composition have no impact on the  
289           drug product performance or inhalation behavior of the patient;  
290           v. Qualitative and/ or quantitative differences in composition do not affect the drug  
291           safety;  
292           vi. The inhaled volume through the device is similar, i.e., 15 % deviation is allowed;  
293           vii. The handling of the device is similar compared to the reference drug product;  
294           viii. The device resistance is similar, i.e., 15 % deviation is allowed;  
295           ix. The target delivered dose (ex-actuator) is similar, i.e., 15 % deviation is allowed.  
296

297 If the formulation differs from that of the comparator product, systemic safety and local  
298 tolerance should be demonstrated.

299

### 300 *Aerodynamic particle size distributions*

301

302 In addition to the above listed criteria, the complete APSD profiles determined by using  
303 validated multistage impactor or impinger methods should be similar. Statistical  
304 assessment of differences should be based on the 90 % confidence interval (CI)  
305 preferably at each individual impactor stage or at grouped stages covering not less than  
306 four relevant groups. A range of up to  $\pm 15\%$  (i.e., 85.0%-115.0% when comparing  
307 arithmetic means or 85.0-117.5% when comparing geometric means) is acceptable.  
308 Justification is required for higher range and this justification usually requires clinical  
309 equivalence data.

310

311 Concerning the extent of the *in vitro* comparison, the following aspect should be  
312 considered when establishing the APSD profiles: -

313

314 i. *Selection of batches:* a minimal number of three batches of the test product  
315 consecutively manufactured and three batches of the reference product should be  
316 used. Due to the possibility of high variability between batches, (at least) three  
317 batches are required to compensate this variability and to provide *in vitro* results that  
318 are representative for the commercial product. If there is high variability within or  
319 between batches, test a large number of batches (and inhalers per batch) of both the  
320 generic product and the comparator product to characterize the variabilities.

321

322 ii. *Each strength:* the *in vitro* studies is performed on each strength proposed for  
323 registration, with and without a spacer (if relevant e.g., pMDI). All aspect of the  
324 spacers needs to be tested i.e., any spacers recommended in the product information  
325 and any spacers described in the product information of the comparator product.

326

327 iii. Flow *rates*: in vitro studies should be performed at an acceptable flow rate range (i.e.,  
328 30 – 90 L/min) taking into consideration the type of product and patient population.  
329 Information on the flow rates, pressure drop ranges and air volumes clinically  
330 applicable to the youngest children should be provided.

331

### 332 3.3.5.2 Step 2: Pulmonary deposition studies

333 If the claim of therapeutic equivalence cannot be supported at the in vitro level, it may be  
334 established by demonstrating equivalent pulmonary deposition along with data that  
335 support the adequate safety of the test product compared to the reference product. This  
336 approach applies to both single API drug products and fixed-dose combination products  
337 that contain more than one API. Regarding equivalent pulmonary deposition, two study  
338 types, namely pharmacokinetic studies and imaging studies, are generally accepted.

339 Pulmonary deposition equivalence studies are usually performed in addition to in vitro  
340 equivalence studies when the generic product, which contains the same active substance  
341 as the comparator product, exhibits differences in excipients, devices, or aerosol  
342 performance characteristics of inhalation products. These studies are also conducted if  
343 the product fails to meet the criteria of the in vitro studies. For more guidance, please  
344 refer to section 6.1 of CPMP/EWP/4151/00 Rev 1.

#### 345 *Pharmacokinetic studies*

346

347 PK studies are used to measure the pulmonary absorption of the inhaled active pharmaceutical  
348 ingredient in the lungs to assess the equivalent efficacy of two drug products. Additionally, PK  
349 studies aim to demonstrate that the test product provides comparable systemic exposure and is  
350 thus equally safe compared to the reference product.

351

352 These PK studies should be conducted in healthy volunteers, although the use of patients  
353 is accepted when justified. When performing PK studies, the following aspects should be  
354 taken into account:

355

356 i. With or without a charcoal block: use a charcoal block if there are data in the  
357 published literature that each pharmaceutical ingredient is fully metabolised in the  
358 first pass and negligible active ingredient can reach the systemic blood circulation  
359 through the gastro-intestinal tract. Studies without active charcoal blockade are  
360 sufficient when absorption of the active ingredient in the lung is very quick (e.g.,  
361  $T_{max} \leq 5$  min) and absorption occurs before the contribution of gastrointestinal  
362 absorption is significant (e.g., salbutamol, salmeterol). In this case, AUC<sub>0-30 min</sub>  
363 is usually acceptable as a surrogate for efficacy and AUC<sub>0-t</sub> for safety;

364

365 ii. Use each strength of the medicine: unless the **in vitro** data justify only testing one  
366 strength, which is when the **in vitro** results of both the reference product and  
367 proposed product are both linear over all the strengths. If only one strength is used,  
368 the highest strength is more preferable; and



369           iii. Dose: at clinically justifiable dose(s) (provide rationale for dose choice): often the  
370           highest therapeutic dose allowed for that strength by the product.

371

372    *Equivalence parameters and criteria*

373    The evaluation of equivalence in PK studies should be based on conventional  
374    bioequivalence criteria, which include the maximum or peak plasma concentration  
375    (C<sub>max</sub>), the area under the plasma concentration curve (AUC), and the time to C<sub>max</sub>  
376    (t<sub>max</sub>). For the primary variables, AUC and C<sub>max</sub>, the two-sided 90% confidence interval  
377    (CI) of the test product (T) and the reference product (R) ratio T/R should fall within the  
378    range of 80.00% - 125.00%.

379    For highly variable active pharmaceutical ingredients, the confidence limits for C<sub>max</sub> can  
380    be widened in line with the requirements prescribed in the Compendium of Guidelines for  
381    Marketing Authorization of Human Medicinal Products: part III, section 3.1.8.

382    *Selection of batches*

383

384    The choice of batches used in the PK studies is critical due to the high variability in  
385    aerodynamic particle size distribution between batches of the reference product and  
386    changes in PSD and delivered dose during storage.

387    Before performing the in vivo comparison, representative batches of the test and  
388    reference products should be established by testing several batches of both products and  
389    selecting batches that are close to the median fine particle dose (or aerodynamic fine  
390    particle dose) for each product.

391    Side batches (batches in the tails of the distribution) representing the test product  
392    specifications can also be used in the PK studies, along with side batches of the reference  
393    product obtained from the market.

394    For fixed-dose combinations, different batches can be used for each component if pre-  
395    specified in the protocol.

396

397    *Imaging studies*

398

399    Lung imaging using gamma scintigraphy with a radiolabeled active pharmaceutical  
400    ingredient is another method to demonstrate equivalent lung deposition between the test  
401    product and the reference product. These studies aim to quantify the regional lung  
402    deposition within different zones of the lungs.

403

404    However, it's important to note that imaging studies have limitations when it comes to  
405    making equivalence decisions. The current OIP guideline clearly states that these studies  
406    cannot replace PK efficacy studies. Instead, the data obtained from imaging studies

407 should serve as supportive evidence for evaluating therapeutic efficacy and should be  
408 complemented by PK studies or clinical studies.

### 409 **3.3.5.3 Step 3: Pharmacodynamic studies**

411  
412 At the final step of the stepwise approach, pharmacodynamic (PD) studies or clinical  
413 studies are necessary when *in vitro* studies and pharmacokinetic (PK) data were  
414 insufficient or failed to demonstrate therapeutic equivalence. These studies aim to provide  
415 evidence that differences in PK do not affect the safety or efficacy of the test product  
416 compared to the reference product.

417  
418 If the approved indication of the reference product covers both asthma and COPD,  
419 therapeutic equivalence studies are only required in one population. It is preferable to  
420 conduct these studies in asthma patients as they are easier to carry out.

421  
422 A key prerequisite for PD efficacy and safety studies is assay sensitivity, which enables  
423 the differentiation of the efficacy and safety of treatments or formulations. Sensitivity is  
424 confirmed when one of the two studied "non-zero" dose levels demonstrates superiority.  
425 Therefore, a minimum of two dose levels should generally be investigated for both  
426 products. It is particularly important that these dose levels are investigated in the steep  
427 part of the dose-response curve to draw reliable and valid conclusions on the therapeutic  
428 equivalence of both products.

429  
430 In the development of orally inhaled products for use in children, adolescents, and adults,  
431 where therapeutic equivalence between two inhaled products must be demonstrated,  
432 pharmacokinetic, pharmacodynamic, and/or clinical studies are likely to be required. Such  
433 studies may be required across the entire age range of the population, and they may need  
434 to be performed separately for each subgroup: less than 2 years, 2-5 years, 6-12 years,  
435 and above 12 years. In this case, the design of the PD studies should reflect the target  
436 population.

## 437 **4. CHANGING THE FORMULATION OR DELIVERY DEVICE**

438  
439  
440 When there is a change in the formulation or delivery device of a nasal spray or inhalation  
441 medicines, the following should be demonstrated: -

- 442 i. The new product is therapeutically equivalent to existing product (when only *in vitro*  
443 equivalence data are required) or acceptable comparator product (when lung  
444 deposition clinical equivalence data are required); and
- 445  
446 ii. The design and principle of operation of the delivery devices for new product and  
447 existing product are the same.

448

449 **4.1 Changes that only require in vitro data**

450

451 Some changes to the formulation or delivery device, therapeutic equivalence may be  
452 demonstrated by using only *in vitro* results: -

453

454 i. Use *in vitro* physicochemical methods such as measurement of aerodynamic  
455 particle size distribution of the old and new products at several flow rates;

456

457 ii. Provide justification for why clinical data are unnecessary if significant physical  
458 differences are observed; and

459

460 iii. Apply the principles used to determine therapeutic equivalence outlined above.

461

462 **4.2 Changes that are likely to modify deposition profile**

463

464 If the deposition profile is likely to be modified by a formulation or delivery device change,  
465 it is necessary to provide *in vitro* physicochemical and lung deposition data, as well as  
466 clinical data, to demonstrate the therapeutic equivalence of the new product with the  
467 comparator product. The following changes may require such data:

468

469 i. Changes to the delivery device that might modify deposition profile; and

470

471 ii. Substantial changes to the formulation, such as changing the concentration or  
472 buffer of a solution, addition of an agent to modify flow or hygroscopic properties  
473 of a powder and removal or substitution of a carrier of a powder.

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490 **5. CHANGE HISTORY**

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<b>Revision No:</b>	<b>Date</b>	<b>Author</b>	<b>Description of change</b>	<b>Section(s) Modified</b>	<b>Approvals</b>
Nil	Nil	Nil	Nil	Nil	Nil

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